

# Optimization and Characterization of Lovastatin Loaded Ufasomes by Definitive Screening Design

B. Naga Bhavana<sup>1</sup>, Pavan Kumar Krosuri<sup>1\*</sup>

<sup>1</sup>Department of Pharmaceutics, Santhiram College of Pharmacy, NH-40, Nandyal- 518112, Andhra Pradesh, India.

\*Corresponding author mail: [pavankumarmph@gmail.com](mailto:pavankumarmph@gmail.com)

## ABSTRACT:

Lovastatin is a lipid-lowering agent belonging to the class of HMG-CoA reductase inhibitors, widely used in the treatment of Hyperlipidemia. Lovastatin was loaded into Ufasomes to enhance its solubility and bioavailability. Reverse phase evaporation method was employed to formulate Lovastatin-loaded ufasomes using a systematic optimization approach. The independent variables considered were oleic acid (mg) (A), cholesterol (mg) (B), stirring speed (rpm) (C), and Surfactant concentration (v/v) (D), and their effects were evaluated on entrapment efficiency (EE%), particle size (nm), and zeta potential (mV). The ufasomal suspension prepared by reverse phase evaporation was subjected to lyophilization, and the obtained powder was further characterized for physicochemical properties. Among all the formulations, the optimized formulation (e.g., UF-4) showed a particle size of 185 nm, zeta potential of -35 mV, and entrapment efficiency of 88%. The optimized formulation exhibited enhanced drug release of 93.50% compared to the pure drug (20.40%). Kinetic studies of the optimized formulation showed the highest R<sup>2</sup> value for the Higuchi model (R<sup>2</sup> = 0.9998), indicating that the drug release follows a diffusion-controlled mechanism.

**Key words:** Lovastatin, Ufasomes, Definitive screening, Reverse Phase Evaporation.

**How to cite this article:** Bhavana BN, Krosuri PK. Optimization and Characterization of Lovastatin Loaded Ufasomes by Definitive Screening Design. *Int J Drug Deliv Technol.* 2026;16(18s): 558-565. DOI: 10.25258/ijddt.16.18s.60

## INTRODUCTION:

Unsaturated fatty acids, like oleic acid, spontaneously form bilayer vesicles in aqueous media, especially in alkaline circumstances, to form ufasomes, innovative vesicular drug delivery methods. These vesicles are adaptable carriers for a variety of medicinal treatments because of their special amphiphilic character, which enables them to encapsulate both hydrophilic medications in their internal water core and lipophilic drugs within the lipid bilayer. By promoting improved absorption across biological membranes, ufasomes increase drug stability, shield medications from deterioration, and boost bioavailability. They are particularly helpful for enhancing patient compliance, lowering the frequency of doses, and controlling and sustaining drug release. Ufasomes are less expensive, simpler to make, and have minimal toxicity and superior biocompatibility when compared to traditional carriers like liposomes. However, the pH of the surrounding environment affects their stability, and the presence of unsaturated bonds makes them vulnerable to oxidative destruction, which may restrict long-term storage. Ufasomes have been used extensively in topical, oral, and transdermal drug delivery systems, especially for medications that improve solubility, permeability, and overall therapeutic efficacy, such as antifungals, anti-inflammatory agents, and lipid-lowering medications like lovastatin.[1-5]

## MATERIALS:

Lovastatin was obtained from Yarrow Chemicals (Mumbai, India). Cholesterol, isopropyl alcohol, oleic acid, and arachidonic acid were procured from Lobe Chemie (Mumbai, India). Sodium oleate was purchased from Ibuy chemicals (Mumbai, India). All reagents were of analytical grade and used as received without further purification.[6-10]

## METHOD OF PREPARATION:

### Reverse Phase Evaporation Method:

Reverse phase evaporation method involves dissolving fatty acids such as oleic acid, arachidonic acid, and sodium oleate along with cholesterol in an organic solvent, isopropyl alcohol, to form the organic phase. Lovastatin is dissolved in distilled water to prepare the aqueous phase. The aqueous phase is added slowly into the organic phase with continuous stirring on a magnetic stirrer to form a water-in-oil emulsion. The mixture is then subjected to probe sonication to obtain a stable emulsion with reduced droplet size. The organic solvent is removed under reduced pressure using a rotary evaporator at controlled temperature, leading to the formation of a gel-like intermediate which upon further evaporation results in the formation of Ufasomal vesicles. The obtained dispersion is further sonicated to reduce particle size and obtain uniform vesicles. The prepared Ufasomes are observed under a binocular microscope for confirmation of vesicle formation and subsequently

## Optimization And Characterization Of Lovastatin Loaded Ufasomes By Definitive Screening Design

subjected to Lyophilization for drying and further characterization.[11-15]

### EXPERIMENTAL DESIGN:

In this current Research work Definitive Screening Design under Response Surface Methodology was used

by taking Independent variables and Dependent variables. The Independent variables are surfactant concentration, cholesterol, organic phase, stirring speed, oleic acid: Arachidonic acid and dependent variables are particle size, entrapment efficiency, zeta potential.

	Factor 1	Factor 2	Factor 3	Factor 4	Factor 5	Response 1	Response 2	Response 3
Run	A: Surfactant concentration	B:Cholesterol	C: Organic Phase	D: Stirring speed	E: Oleic acid: Arachidonic acid	Particle Size	Entrapment Efficiency	Zeta potential
	w/v	w/w	v	RPM	w/w	nm	%	mV
1	1	10	30	1250	3:1	195	83	-38
2	5	10	17.5	500	3:1	241	73	-30
3	5	50	5	1250	1:1	280	68	-32
4	1	30	30	500	1:1	190	86	-33
5	5	30	5	2000	3:1	285	66	-37
6	3	30	17.5	1250	3:1	243	74	-37
7	5	50	30	500	3:1	281	64	-31
8	3	50	30	2000	3:1	276	67	-39
9	1	10	5	2000	1:1	193	88	-38
10	3	30	17.5	1250	1:1	232	78	-33
11	1	50	17.5	2000	1:1	233	79	-38
12	5	10	30	2000	1:1	259	72	-30
13	1	50	5	500	3:1	216	80	-40
14	3	10	5	500	1:1	198	85	-31

# Optimization And Characterization Of Lovastatin Loaded Ufasomes By Definitive Screening Design

## Calibration curve:

Prepare a series of standard solutions of known concentrations and measure their absorbance using a suitable analytical instrument UV–vis spectrophotometer Plot absorbance versus concentration to obtain a calibration curve and use it to determine unknown sample concentrations.[16,17]

## FT-IR:

The sample is prepared (e.g., mixed with KBr and compressed into a pellet or placed directly on the ATR crystal) and exposed to infrared radiation in an FTIR spectrophotometer. The instrument records the absorption spectrum, which is used to identify functional groups and characterize the sample.[18-20]

## Particle Size:

The particle size of ufasomes is determined by diluting the vesicle dispersion with distilled water and analyzing it using dynamic light scattering (DLS) in a particle size analyzer. The instrument measures the mean vesicle diameter and size distribution based on light scattering patterns.[21-24]

## Zeta potential:

The zeta potential of ufasomes is measured by diluting the vesicle dispersion with distilled water and analyzing it using a zeta potential analyzer based on electrophoretic mobility. It indicates the surface charge of vesicles, which helps predict stability and aggregation behavior.[25,26]

## Entrapment Efficiency:

Entrapment efficiency of Ufasomes is determined by separating the untrapped (free) drug from vesicles using centrifugation or dialysis. The amount of entrapped drug is quantified by UV–Vis Spectro photometry and expressed as a percentage of the total drug used.[26-28]

## X-Ray Diffraction:

The Ufasome sample is Lyophilized, finely powdered, and placed in the sample holder of an X-ray diffractometer. The diffraction pattern is recorded over a suitable  $2\theta$  range to determine crystallinity and possible drug–excipient interactions. [28]

## Diffraction Scanning Calorimetry (DSC):

The lyophilized Ufasomes sample is accurately weighed, sealed in an aluminum pan, and placed in a Differential Scanning Calorimeter. The sample is heated at a controlled rate to record thermograms, which reveal phase transitions and drug–excipient interactions. [28,29]

## Transmission electron microscopy (TEM):

A drop of diluted Ufasomes dispersion is placed on a carbon-coated copper grid, stained with phospho tungstic acid, and allowed to dry. The sample is then observed under a transmission electron microscope to study vesicle size, shape, and morphology. [28-30]

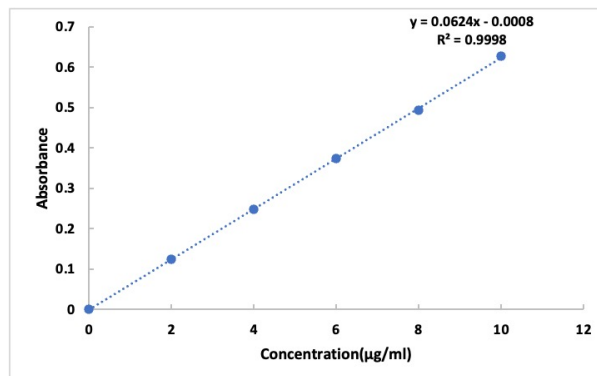


Fig: No.1 Standard Calibration Curve of Lovastatin

The calibration curve of Lovastatin shows a linear increase in absorbance with concentration, following the Beer–Lambert law. The high  $R^2$  value (0.9998) indicates excellent accuracy and reliability for quantitative analysis.

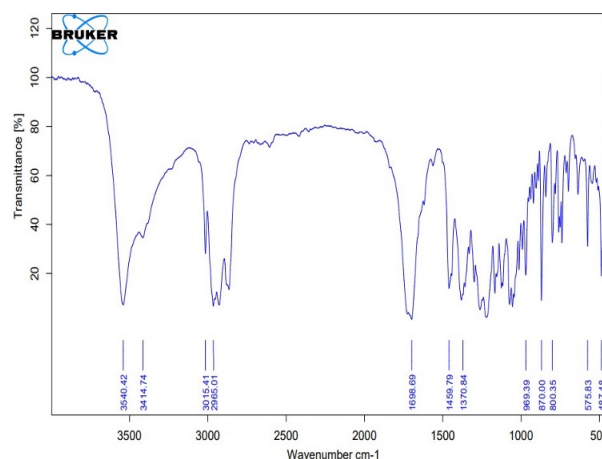


Fig: No.2 FT-IR Spectra of Optimized Lovastatin loaded Ufasomes

The FT-IR spectrum of lovastatin shows characteristic peaks confirming its functional groups and structural integrity. The broad band around  $3015\text{ cm}^{-1}$  indicates O–H stretching, while peaks at  $2950\text{--}2850\text{ cm}^{-1}$  correspond to aliphatic C–H stretching. A strong peak near  $1700\text{--}1735\text{ cm}^{-1}$  represents C=O stretching of ester/lactone groups, and bands in the range of  $1600\text{--}1450\text{ cm}^{-1}$  indicate C=C vibrations. Peaks between  $1250\text{--}1050\text{ cm}^{-1}$  are due to C–O stretching. The absence of significant peak shifts suggests that the drug is stable and shows no chemical incompatibility.

# Optimization And Characterization Of Lovastatin Loaded Ufasomes By Definitive Screening Design

Table 1: ANOVA results of the response variable of Experimental Design

Source	Particle Size (R1)				Entrapment Efficiency (R2)			
	Sum of Squares	Mean Square	F-value	p-value	Sum of Squares	Mean Square	F-value	p-value
Model	16056.36	1784.0	14219.	<0.0001	820.79	91.20	2672.45	<0.0001
A-Surfactant concentration	9207.28	9207.2	73384.	<0.0001	458.64	458.64	13439.6	<0.0001
B-Cholesterol	3471.11	3471.1	27665.	<0.0001	145.89	145.89	4275.03	<0.0001
C-Organic Phase	32.41	32.41	258.30	<0.0001	11.31	11.31	331.51	<0.0001
D-Stirring speed	1655.11	1655.1	13191.	<0.0001	39.50	39.50	1157.59	<0.0001
E-Oleic acid:	355.56	355.56	2833.9	<0.0001	54.52	54.52	1597.51	<0.0001
Arachidonic acid								
A <sup>2</sup>	0.0806	0.0806	0.6423	0.4678	0.0411	0.0411	1.20	0.3340
B <sup>2</sup>	0.2368	0.2368	1.89	0.2414	0.0411	0.0411	1.20	0.3340
C <sup>2</sup>	0.0806	0.0806	0.6423	0.4678	0.0411	0.0411	1.20	0.3340
D <sup>2</sup>	0.2368	0.2368	1.89	0.2414	0.3224	0.3224	9.45	0.0372
Residual	0.5019	0.1255			0.1365	0.0341		
Cor Total	16056.86				820.93			

Zeta potential (R3)

Source	Zeta potential (R3)			
	Sum of Squares	Mean Square	F-value	p-value
Model	174.00	19.33	214.85	<0.0001
A-Surfactant concentration	92.90	92.90	1032.4	<0.0001
B-Cholesterol	7.90	7.90	87.83	0.0007
C-Organic Phase	11.65	11.65	129.50	0.0003
D-Stirring speed	42.59	42.59	473.32	<0.0001
E-Oleic acid:	48.80	48.80	542.36	<0.0001
Arachidonic acid				
A <sup>2</sup>	0.2368	0.2368	2.63	0.1800
B <sup>2</sup>	0.2368	0.2368	2.63	0.1800
C <sup>2</sup>	1.11	1.11	12.36	0.0246
D <sup>2</sup>	0.2368	0.2368	2.63	0.1800
Residual	0.3599	0.0900		
Cor Total	174.36			

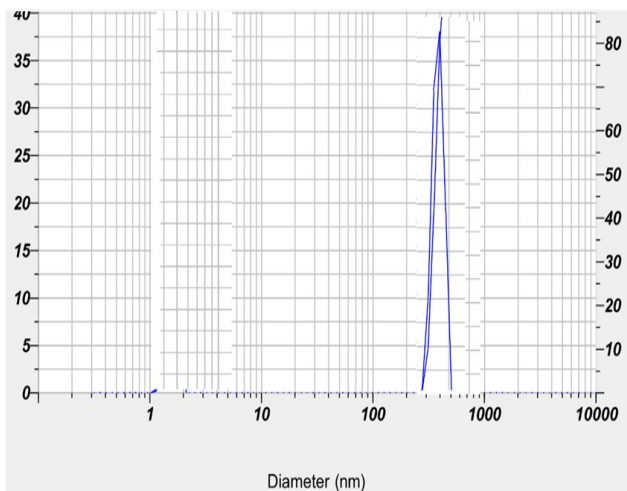
Equation

$$Y_1 = 237.47 + 30.83A + 18.93B + 1.83C + 13.07D + 5.35E + 0.1842A^2 - 0.3158B^2 + 0.1842C^2 - 0.3158D^2$$

$$Y_2 = 75.95 - 6.88A - 3.88B - 1.08C - 2.02D - 2.10E - 0.1316A^2 - 0.1316B^2 - 0.1316C^2 + 0.3684D^2$$

$$Y_3 = -34.97 + 3.10A - 0.9032B + 1.10C - 2.10D - 1.98E + 0.3158A^2 + 0.3158B^2$$

quadratic terms show non-linear effects: A<sup>2</sup>, B<sup>2</sup>, and D<sup>2</sup> (positive) enhance zeta potential at higher levels, while C<sup>2</sup> (negative) reduces it due to curvature influence.



### From ANOVA table the model is significant Effect of Independent Variables Vs Response Y1(Particle size)

The given equation represents a polynomial regression model used to predict particle size based on formulation variables (A, B, C, D, and E). The constant (237.47) indicates the baseline particle size, while coefficients of A–E show how each factor influences particle size (positive values increase size, negative values decrease it). The quadratic terms (A<sup>2</sup>, B<sup>2</sup>, C<sup>2</sup>, D<sup>2</sup>) indicate non-linear effects, meaning changes in these variables can have curvature impact on particle size rather than a simple linear relationship.

### Effect of Independent variables Vs Response Y2(Entrapment Efficiency)

The equation represents a quadratic regression model where the baseline entrapment efficiency is 75.95, and negative coefficients of A–E indicate that increasing these factors decreases entrapment efficiency. Quadratic terms show non-linear effects, with A<sup>2</sup>, B<sup>2</sup>, and C<sup>2</sup> reducing efficiency at higher levels, while D<sup>2</sup> has a positive influence, indicating improvement at higher concentrations.

### Effect of Independent variables Vs Response Y3(Zeta Potential)

The equation represents a quadratic regression model for predicting zeta potential based on formulation variables (A–E). The constant (–34.97) indicates the baseline zeta potential, while A and C (positive coefficients) increase zeta potential, whereas B, D, and E (negative coefficients) decrease it. The

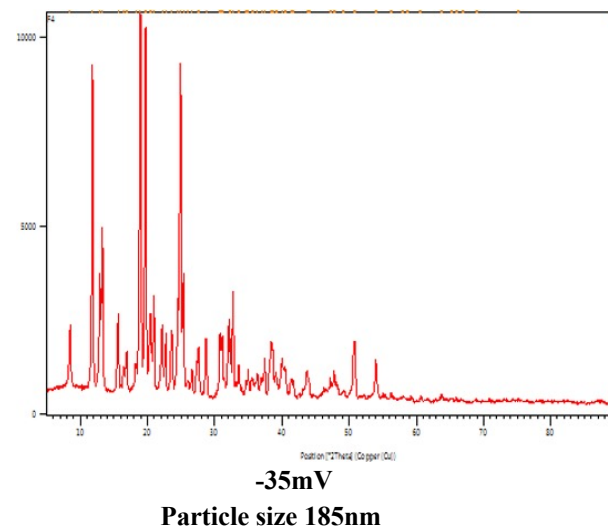
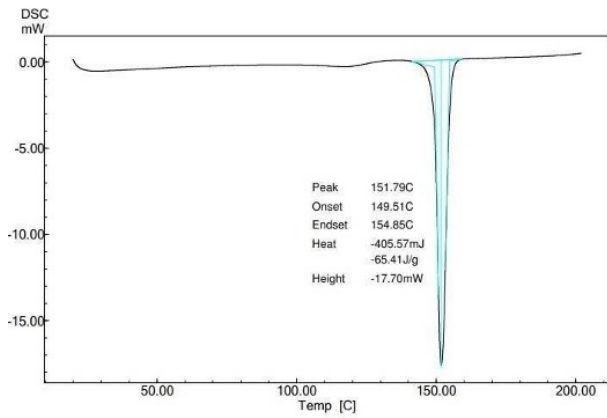


Fig: No.3 Zeta Potential and Particle Size of Optimized Formulation

# Optimization And Characterization Of Lovastatin Loaded Ufasomes By Definitive Screening Design

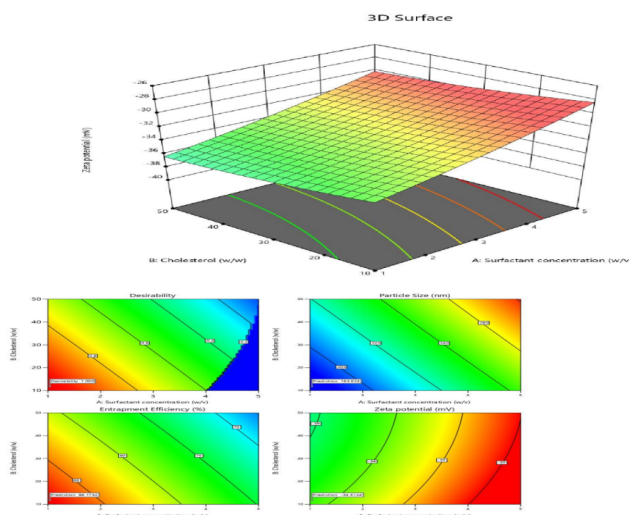


A)  
B)

**Fig: No.4 DSC STUDIES of A) Pure drug, B) Optimized formulation (OPLU1)**

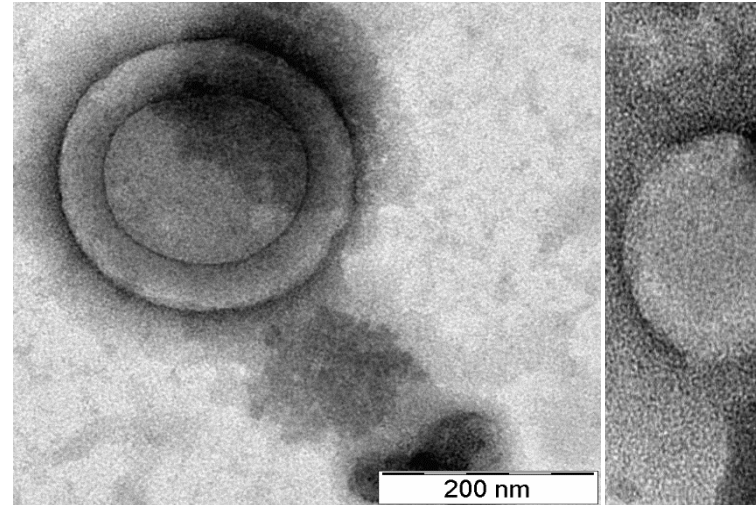
**DSC Studies:** Reduction in Melting points from 151°C to 127 °C from pure Drug to Optimized Formulation in DSC peaks indicates decrease in crystallinity and increase in solubility.

A)  
B)

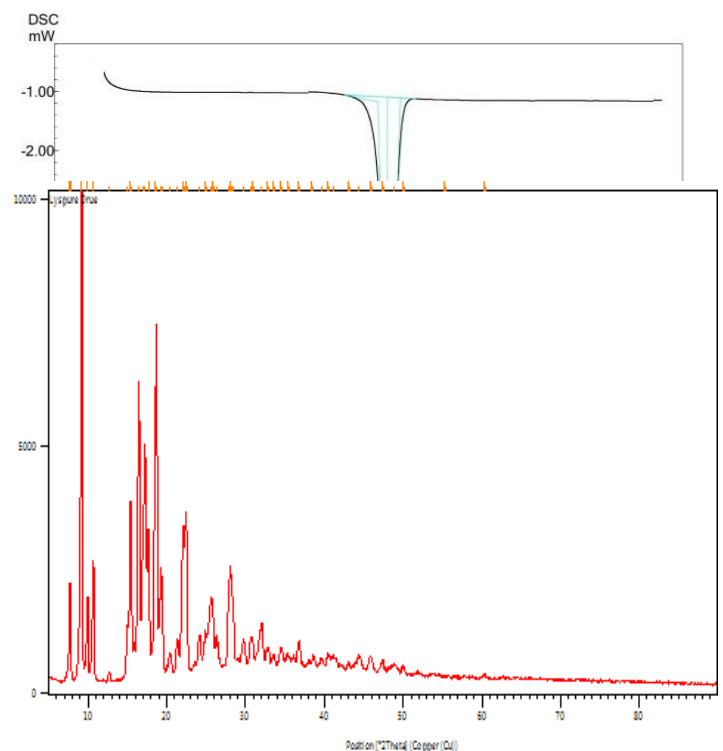


**Fig: No.5 XRD STUDIES Of A) Pure Drug, B) Optimized Formulation**

**XRD Studies:** Reduction in Peak Intensities in XRD peaks from pure Drug to Optimized Formulation indicates decrease in crystallinity and increase in solubility.



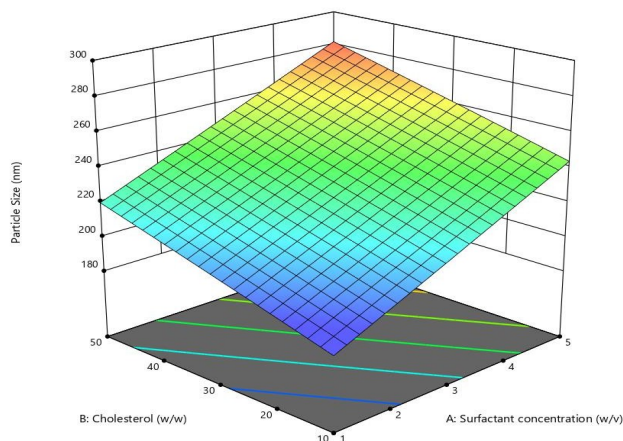
**Fig: No. 6 TEM Images of Optimized Formulation (OPLU1)**



# Optimization And Characterization Of Lovastatin Loaded Ufasomes By Definitive Screening Design

A)

3D Surface

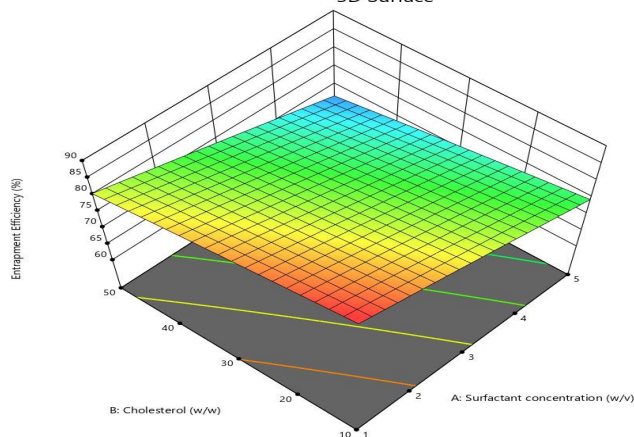


B)

C)

The data shows that the optimized formulation releases the drug much faster and in higher amounts compared to the pure drug over 6 hours. While the

3D Surface



optimized formulation reaches about 93% drug release, the pure drug releases only around 20%. This means the optimized formulation improves drug release and works more effectively, showing a steady and controlled release pattern.

**Kinetic Study:** To Know drug release kinetics of the optimized formulation of the dissolution were subjected to different Kinetic models such as Zero order, First order, Higuchi, Korsmeyer peppasetc...

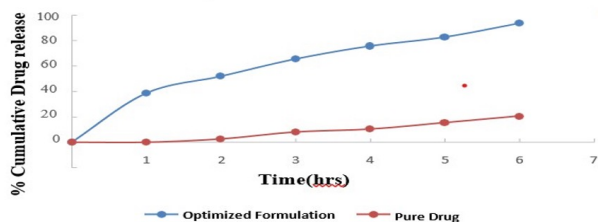
**Table.NO.2 Kinetic Studies of Optimized Formulation OPLU1**

Formulation code	Zero order R <sup>2</sup>	First order R <sup>2</sup>	Higuchi model R <sup>2</sup>	Korsmeyerpeppas model	
				R <sup>2</sup>	n
OPLU1	0.924	0.964	0.997	0.503	1.5

From the above observations Kinetic analysis (R<sup>2</sup>) of release data based on best curve fitting method for Lovastatin loaded Ufasomes, R<sup>2</sup> value is more for Higuchi model i.e., R<sup>2</sup>= 0.9979 indicating that the drug release from Ufasomal carrier is based on Fickian diffusion, predicting that the rate of drug release is proportional to the square root of time.

## CONCLUSION:

Lovastatin, a BCS class II medication used to treat hyperlipidemia, has a low oral bioavailability of 5%. To get over its solubility problems, it acts on an HMG CoA reductase inhibitor. Ufasomes were loaded with lovastatin as nanocarriers. The Definitive screening design was used to optimize the Lovastatin-loaded Ufasomes. Oleic acid, Arachidonic acid, stirring speed, and cholesterol were considered independent factors, while particle size, Zeta potential, and entrapment efficiency were



**Fig: No. 7 3D SURFACE PLOT OF RESPONSE OF A) Particle size (Y1), B) Entrapment Efficiency(Y2), C) Zeta Potential (Y3).**

# Optimization And Characterization Of Lovastatin Loaded Ufasomes By Definitive Screening Design

considered dependent variables. The Lovastatin-loaded Ufasomes were prepared using the reverse phase evaporation method, and then they were characterized using DSC, XRD, and TEM analysis. Among fourteen formulations obtained through Definitive screening design, OPLU-1 was chosen as an optimized formulation with less particle size of 185 nm, and maximum entrapment efficiency of 88 %. In vitro dissolution studies were conducted for both the optimized formulation and the pure drug (lovastatin). A comparison of the dissolution profiles of the optimized formulation and the pure drug. The optimized formulation revealed a maximum drug release of 93.35% within 6 hours, which is greater solubility and drug release. For the optimized formulation (OPLU- 1), kinetic studies such as zero order, first order, Higuchi, and korsmeyer pepas were conducted. The results showed that the Higuchi model had a maximum R square value of 0.997, indicating that the drug release from the carrier is based on Fickian diffusion, predicting that the rate of drug release is proportional to the square root of time.

## ACKNOWLEDGEMENT:

The authors wish to express their sincere gratitude to Department of Pharmaceutics, Santhiram College of Pharmacy, Nandyal (Dt), Andhra Pradesh, India for providing necessary facilities to carry out this research work.

## CONFLICT OF INTEREST

We declare that we have no conflict of interest.

## REFERENCES:

- 1) Torchilin VP. Multifunctional nanocarriers. *Nat Rev Drug Discov.* 2005;4(2):145–160.
- 2) Sahu MK, Tiwari SP. Phytochemical and Ethnopharmacological Review of *Aegle marmelos* Linn. (Bael). *Bulletin of Pioneering Researches of Medical and Clinical Science.* 2024;29-47.
- 3) Verma S, Singh SK, Syan N, Mathur P, Valecha V. Nanoparticle vesicular systems: a versatile tool for drug delivery. *J Chem Pharm Res.* 2010 Jan 1;2(2):496-509.
- 4) Jain S, Jain V, Mahajan SC. Lipid based vesicular drug delivery systems. *Advances in Pharmaceutics.* 2014;2014(1):574673.
- 5) Jadhav SM, Morey P, Karpe MM, Kadam V. Novel vesicular system: an overview. *Journal of applied pharmaceutical science.* 2012 Jan 30:193-20.
- 6) Alenzi AM, Albalawi AE, Alharbi KS, Alzahrani KJ. Review on different vesicular drug delivery systems (VDDSs) and their applications. *Recent Pat Nanotechnol.* 2023;17(1):1–12.
- 7) Biju SS, Talegaonkar S, Misra PR, Khar RK. Vesicular systems: an overview. *Indian J Pharm Sci.* 2006;68(2):141–53.
- 8) Mittal R, Sharma A, Arora S. Ufasomes mediated cutaneous delivery of dexamethasone: formulation and evaluation of anti-inflammatory activity by carrageenin-induced rat paw edema model. *J Pharm (Cairo).* 2013;2013:680580.
- 9) Sharma A, Arora S. Formulation and in vitro evaluation of ufasomes for dermal administration of methotrexate. *ISRN Pharm* 2012;2012:873653.
- 10) Arundhasree R, Rajalakshmi R, Aiswarya R, Rajendra Kumar A, Kumar SS, Nair SC. Ufasomes: unsaturated fatty acid based vesicular drug delivery system. *Int J Appl Pharm.* 2021;13(2):76–83.
- 11) Salama AH, Aburahma MH. Ufasomes nano-vesicles-based lyophilized platforms for intranasal delivery of cinnarizine: preparation, optimization and evaluation. *Pharm Dev Technol.* 2016;21(6):706–15.
- 12) Hargreaves WR, Deamer DW. Liposomes from ionic, single-chain amphiphiles. *Biochemistry.* 1978;17(18):3759–6
- 13) Adams SP, Alaeiikhchi N, Wright JM. Lovastatin for lowering lipids. *Cochrane Database Syst Rev.* 2023;3:CD014858.
- 14) Gold ME, Nanna MG, Doerfler SM, Schibler T, Wojdyla D, Peterson ED, et al. Prevalence, treatment, and control of severe hyperlipidemia. *Am J Prev Cardiol.* 2020;3:100079.
- 15) Stancu C, Sima A. Statins: mechanism of action and effects. *J Cell Mol Med.* 2001;5(4):378–87.
- 16) Sirtori CR. Pharmacology and mechanism of action of the new HMG-CoA reductase inhibitors. *Pharmacol Res.* 1990;22(5):555–63.
- 17) Shreya k, J baser, Ufasome; A comprehensive review of design, characterization and applications. *World Journal of Advanced Research and Review,* 2025,26(03),2302-2311.
- 18) Ghantasala Elizabeth Prashanthi, Ufasomes; Unveiling the potential of vesicular drug delivery system, *International Journal of Pharmaceutical Research and Applications,* 2025, Vol 10, 1205-1213.
- 19) Sara M. Hasheem, Itraconazole - Loaded Ufasomes; Evaluation, characterization, and Anti-

## Optimization And Characterization Of Lovastatin Loaded Ufasomes By Definitive Screening Design

Fungal Activity against *Candida albicans*,  
*Pharmaceutics* 2023,15,26.

20) Sara M. Hasheem, Itraconazole- Loaded Ufasomes; Evaluation, characterization, and the Anti-Fungal Activity against *Candida albicans*,  
*Pharmaceutics*2023,15,26.

21) Bassant Atef, 10- Hydroxy Decanoic Acid-Based Vesicles as a Novel Topical Delivery System; Would It Be a Better Platform than Conventional Oleic Acid Ufasomes for Skin cancer Treatment,  
*Pharmaceutics*, 2023,15,1461.

22) ) Harshil M. Patel, A Vesicular Drug Delivery for Futuristic Drug Delivery Applications,  
*India J. Pharm. Biol. Res.*2022;10(4);1-3

23) Navjot Singh, Ufasomes; An Emerging Vesicular System and A Comparative Study with other Vesicular Carrier,  
*Int.J.Pharm.Sci.Res.*2022,74(2),21.

24) Sree Lakshmi v, Formulation and Evaluation of Ufasomal Topical Gel Containing Selected NonSteroidal Anti-Inflammatory Drug, *J. Pharm. Sci.Res.*Vol.13(1),2021,38-48.

25) Sankha Bhattacharya, Preparation and Characterization of Glyceryl Oleate Ufasome of Terbinafine Hydrochloride: A novel approach to trigger *Candida albicans* fungal infection; *Future Journal of Pharmaceutial Sciences*,2021(7;3),1186

26) Al-Mahmood S, Ayash NR. Ufasomes as topical/transdermal drug delivery system: structural components, preparation techniques and therapeutic application. *Curr Drug Deliv.* 2025;22(8):1047–57.

27) Luke PM, Joseph T. Ufasomes: rising technology for delivery of drugs. *Int J Med Pharm Sci.* 2021;11(11):1–7.

28) Ali MH, Kirby DJ, Mohammed AR, Perrie Y. Solubilisation of drugs within liposomal bilayers: alternatives to cholesterol as a membrane stabilising agent. *J Pharm Pharmacol* 62:1646

29) Chen C-C, Tsai T-H, Huang Z-R, Fang J-Y. Effects of lipophilic emulsifiers on the oral administration of lovastatin from nanostructured lipid carriers: physicochemical characterization and pharmacokinetics. *Eur J Pharm Bio pharm* 74:474–82.

30) Hashem SM, Gad MK, Anwar HM, Saleh NM, Shamma RN, Elsherif NI. Itraconazole-loaded ufasomes: evaluation, characterization, and antifungal activity against *Candida albicans*. *Pharmaceutics.* 2023;15(1):26.